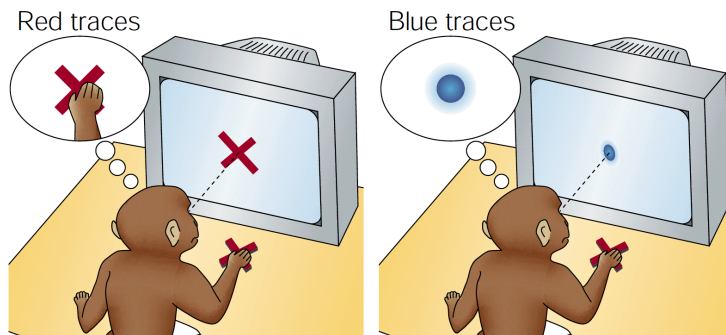


## Attention



Top-down attention: Information in working memory selectively enhances neural representations of sensory stimuli [Desimone01].

### Top-down

- Goal-directed
- Relevant stimuli

### Bottom-up

- Stimulus-driven
- Salient stimuli

### Neuronal signatures

- Enhanced sensitivity
- Enhanced selectivity

### Network signatures

- Enhanced gamma rhythms
- Enhanced spike synchrony

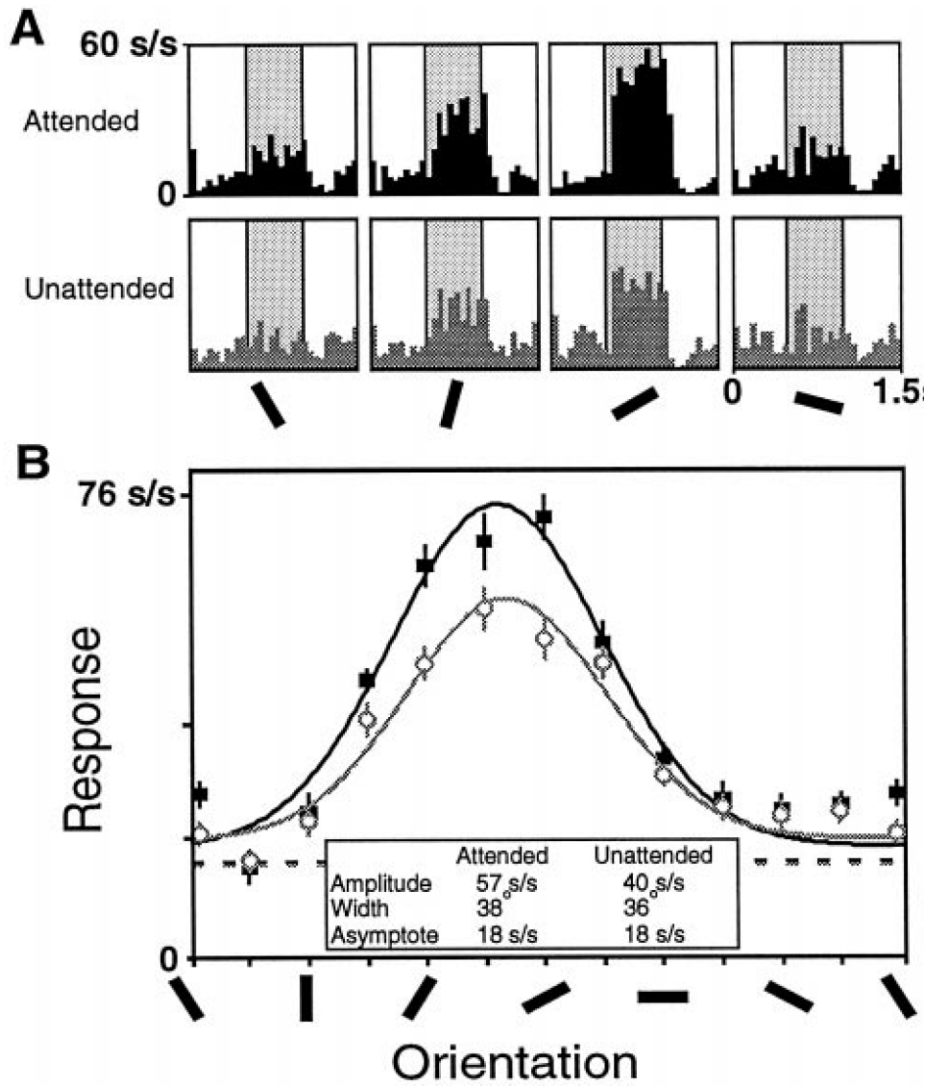
# Macaque brain

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Visual areas in the macaque brain.

Navigation controls: back, forward, and search icons, followed by the text "3 of 10".

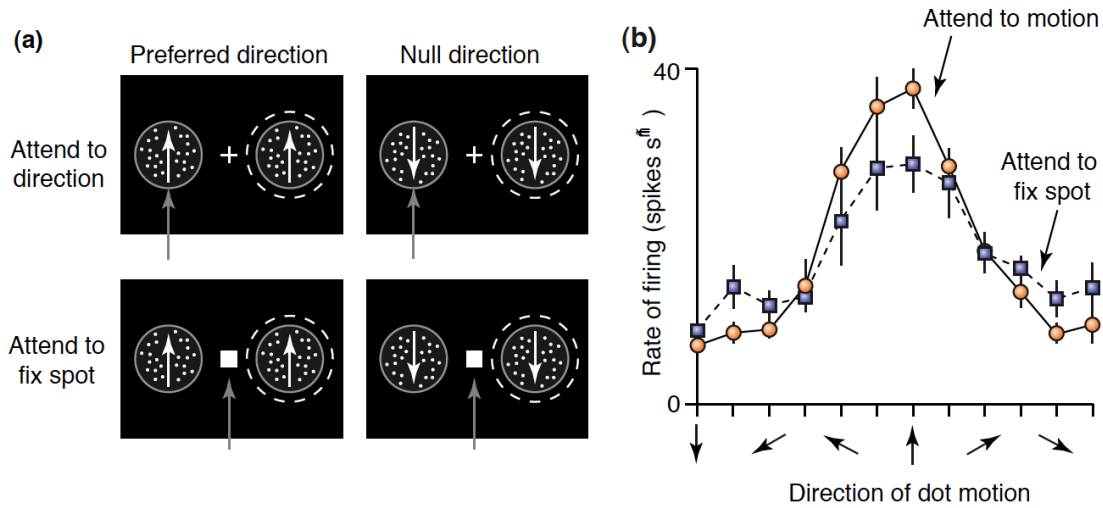
## Visual Cortex (V4): Spatial attention



Recordings from a V4 cell showing enhanced responses in the attended mode (black) relative to the unattended mode (gray). Spike rates are affected multiplicatively [Maunsell 1999].



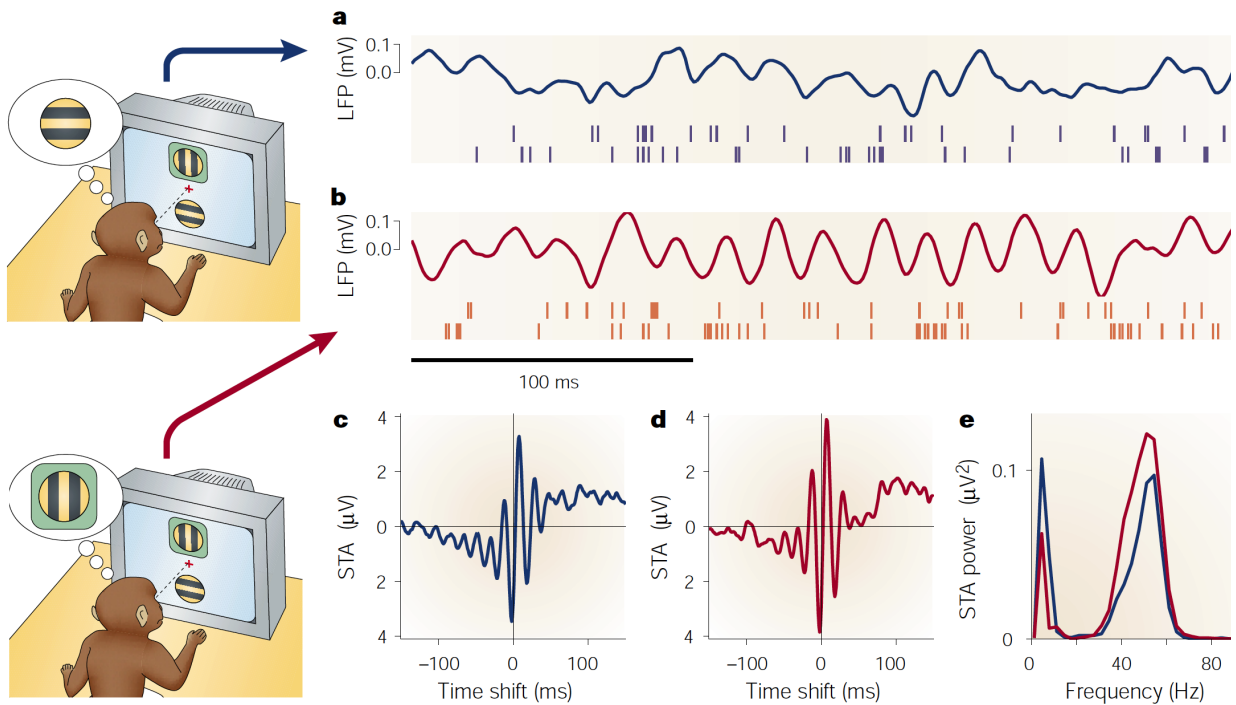
# Visual Cortex (MT): Feature attention



Attention to the neuron's preferred direction of motion increased the neuron's response, but attention to the null direction of motion decreased its response. Thus, attention to a particular direction of motion does not increase responses across all neurons. Rather, it has a push-pulleffect that increases responses only for neurons that prefer motion close to the attended direction [Treue06].

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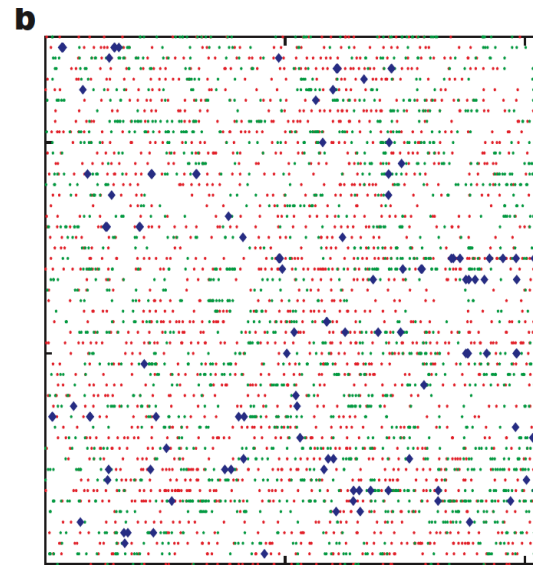
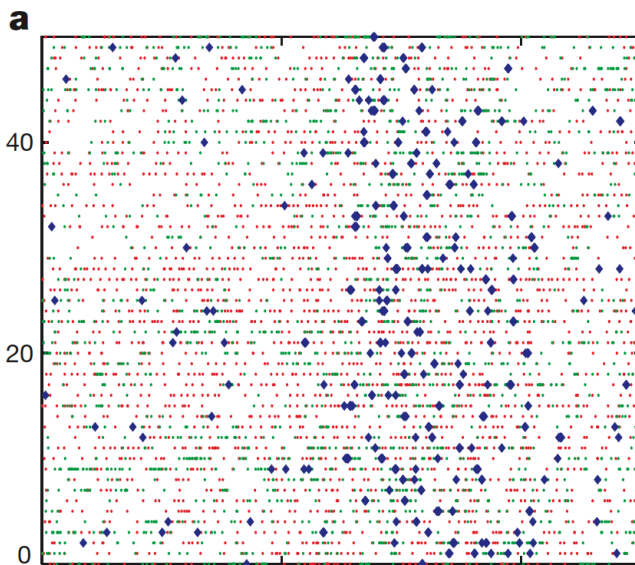
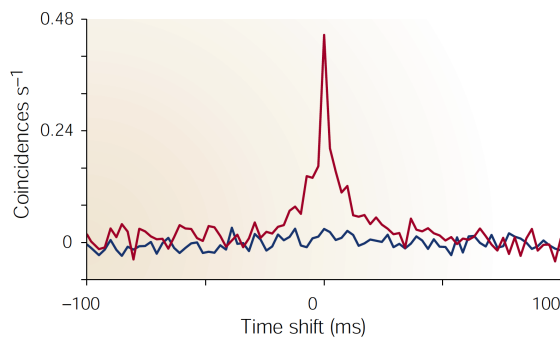
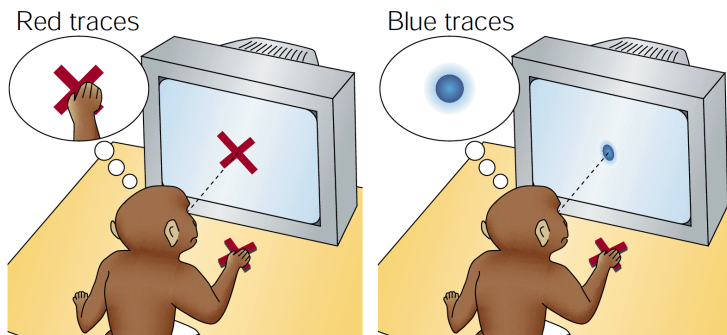
# Visual cortex (V4): Gamma increases



Simultaneously recorded spikes and local field potential (LFP) with attention directed inside (red) or outside (blue) the cell's receptive field. The LFPs' spike-triggered averages (STA) and the STAs' power spectra were computed [Sejnowski01,Steinmetz00].

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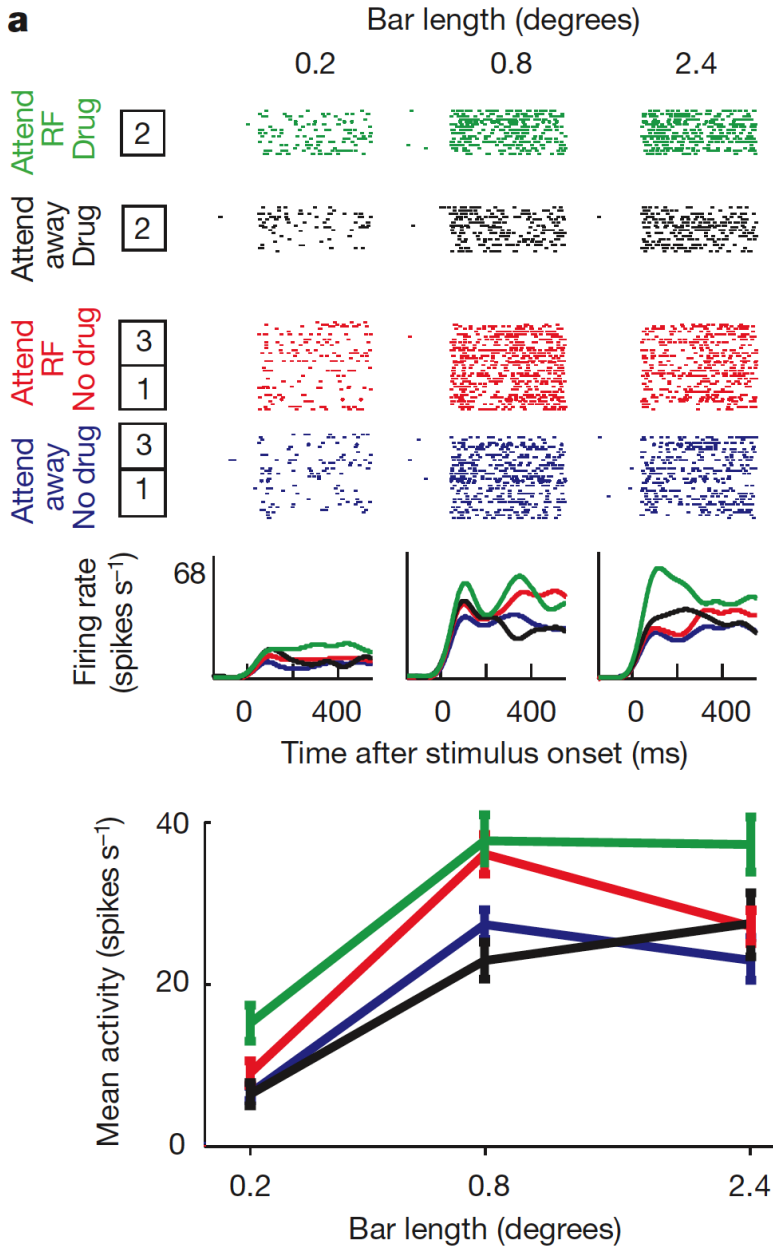
## Somatosensory cortex (SII): Synchrony increases



Spike trains recorded from a pair of neurons (red and green) in secondary somatosensory cortex with (a) and without (b) attention. Synchronous spikes (within 2.4ms) are indicated (blue) and quantified in the cross-correlation histogram above,

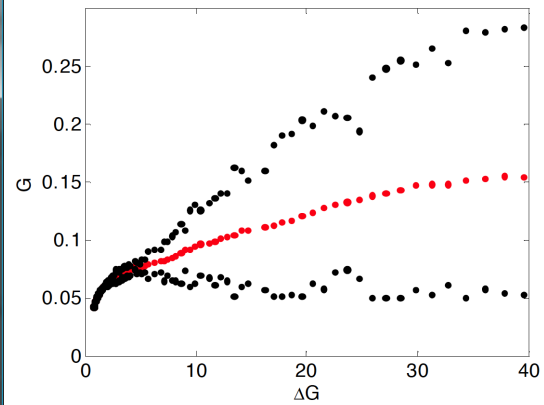
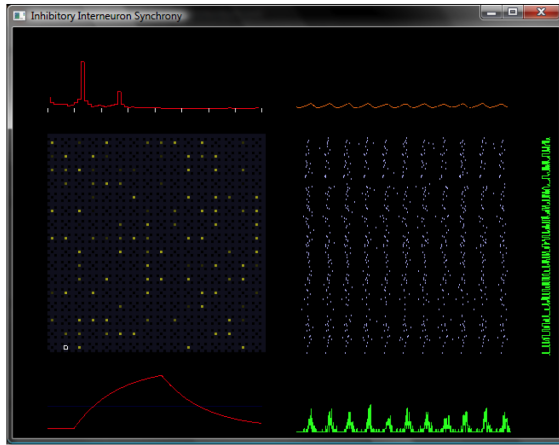
with (red) and without (blue) attention (excess over Poisson) [Sejnowski01,Steinmetz00].

## Cholinergic modulation



Acetylcholine enhances the effect of attention (green – black vs red - blue) in V1; bars of various lengths were presented [Thiele08]. It may act by enhancing both excitatory and inhibitory synaptic transmission, as has been shown *in vitro*.

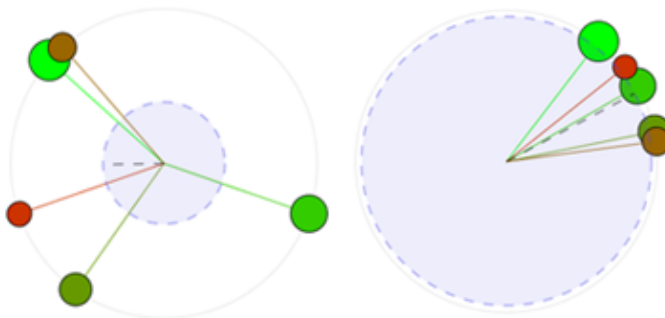
## Controlling synchrony



When inhibition's strength ( $\Delta G$ ) surpasses a critical level, synchrony appears (*left, demo; right,  $G_{\max}$ ,  $G_{\min}$ , and  $\langle G \rangle$  over a cycle versus  $\Delta G$* ). Rate-based models predict that synchrony appears when the loop-gain exceeds unity (i.e.,  $m s > 1$ , where  $m$  and  $1/s$  are the  $A(G)$  and  $G(A)$  curves' slopes, respectively). However, these models ignore heterogeneity, which makes synchrony more difficult to achieve.

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## Kuramoto model addresses heterogeneity



Phases of coupled oscillators with weak (left) and strong (right) coupling. Color and ball-size indicate the oscillators' different intrinsic frequencies; dashed circle and marker indicate the order parameter's magnitude and phase (i.e., vector strength).

Read tutorial: <http://tutorials.siam.org/dsweb/cotutorial/index.php?s=4&p=0>  
 Download Java applet: <http://www.johnwordsworth.com/tutorials/Kuramoto/media/applet/Kuramoto.jnlp>

Instead of pulse-coupling, this model uses phase-coupling:

$$\dot{\theta}_i = \omega_i + \frac{K}{N} \sum_{j=1}^N \sin[\theta_j - \theta_i], \quad i = 1 \dots N$$

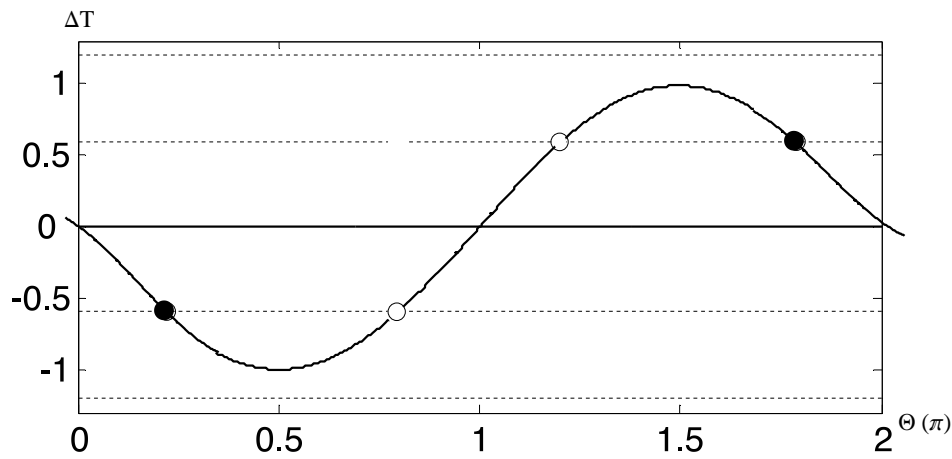
Instead of vector strength, an order parameter is defined:

$$r e^{i\psi} = \frac{1}{N} \sum_{j=1}^N e^{i\theta_j}, \quad i = 1 \dots N$$



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## Relating coupling strength ( $K$ ) to the PRC



The Kuramoto model's sinusoidal phase-coupling corresponds to a PRC that is a flipped sinusoid. To obtain the Kuramoto model's coupling strength,  $K$ , we must multiply the PRC's maximum advance/delay,  $\Delta T_{\max}$ , by the network's total spike rate.

Consider only the  $j^{\text{th}}$  oscillator's effect on the  $i^{\text{th}}$  oscillator:

$$\dot{\theta}_i = \dots + \frac{K}{N} \sin[\theta_j - \theta_i] + \dots$$

If the  $i^{\text{th}}$  oscillator's phase is  $\Theta$  when the  $j^{\text{th}}$  oscillator's phase is 0 — which, by definition, is when it spikes — then we have  $\theta_i = \Theta + \theta_j$ , or  $\theta_j - \theta_i = -\Theta$ . This assumes that the phase-difference remains constant throughout that cycle. In which case, the total change in the  $i^{\text{th}}$  oscillator's phase over the complete cycle — which, by definition, is the PRC — will be:

$$\text{PRC}[\Theta] = \int_0^T \dot{\theta}_i dt = \int_0^T \frac{K}{N} \sin[-\Theta] dt = -T \frac{K}{N} \sin[\Theta]$$

Hence, this model assumes the PRC is a flipped sinusoid. The PRC's maximum delay/advance,  $\Delta T_{\max}$ , is related to the coupling strength,  $K$ , by

$$\begin{aligned} \Delta T_{\max} &= T K / N \\ \Leftrightarrow K &= N \Delta T_{\max} / T \end{aligned}$$

Hence, we must multiply the PRC's amplitude — or inhibition's synaptic strength ( $\Delta G$ ) — by the network's total firing rate to convert it into the Kuramoto model's coupling strength ( $K$ ).